Having thus described the preferred embodiments, the invention is now claimed to be:

1. A method for calibrating a coincidence imaging system which includes a plurality of radiation detectors, the method comprising:

measuring a plurality of coincidence radiation events associated with a point radiation source;

assigning initial values for a set of fitting parameters;

applying a minimization algorithm including:

calculating lines of response (LOR) based upon the fitting parameters and the measured radiation events,

generating a figure of merit characterizing the apparent size of the point radiation source based upon the LOR's, and

optimizing the fitting parameters to produce a minimized figure of merit; and

extracting from the optimized fitting parameters a correction factor relating to a positional coordinate of a detector.

2. A method for imaging using a plurality of radiation detectors, the method comprising:

measuring a plurality of coincidence radiation events associated with a point radiation source;

assigning initial values for at least one fitting parameter;

calculating lines of response (LOR) based upon the at least one fitting parameter and the measured radiation events;

generating a figure of merit characterizing the apparent size of the point radiation source based upon the LOR's;

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optimizing the at least one fitting parameter using a minimization algorithm which includes iteratively repeating the calculating and generating steps to produce a minimized figure of merit;

extracting from the at least one optimized fitting parameter at least one correction factor;

acquiring a set of radiation data from an associated subject;

correcting the radiation data for camera misalignment by correcting the spatial coordinates of the detected radiation events using the at least one correction factor; and

reconstructing an image representation from the corrected radiation data.

- 3. The imaging method as described in claim 2, wherein the at least one fitting parameter includes:
  - a parameter related to the radial positional coordinate of a detector.
- 4. The imaging method as described in claim 2, wherein the at least one fitting parameter includes:
  - a parameter related to the tangential positional coordinate of a detector.
- 5. The imaging method as described in claim 2, wherein the at least one fitting parameter includes:
  - a parameter related to the orientational positional coordinate of a detector.
  - 6. The imaging method as described in claim 2, wherein:
- 30 the step of generating a figure of merit includes summing a distance of closest approach of each LOR to a spatial point; and

the at least one fitting parameter includes the positional coordinates of the spatial point.

- 7. The imaging method as described in claim 2, wherein:
- the step of generating a figure of merit includes summing the square of a distance of closest approach of each LOR to a spatial point; and the at least one fitting parameter includes the
  - the at least one fitting parameter includes the positional coordinates of the spatial point.
- 10 8. The imaging method as described in claim 7, wherein the step of generating a figure of merit further includes:
  - discarding LOR's whose distance of closest approach is greater than a preselected distance.
  - 9. The imaging method as described in claim 2, wherein the step of generating a figure of merit further includes:
    - obtaining a crossing point of each pair of LOR's; and calculating a standard deviation of the crossing points.
  - 10. The imaging method as described in claim 2, wherein the step of generating a figure of merit further includes:
    - obtaining a distance of closest approach for each pair of LOR's; and
    - calculating a standard deviation of the obtained distances.
  - 11. The imaging method as described in claim 2, wherein the number of detectors is N and the fitting parameters include:
    - $\Delta r_i$ , i=1 to N, where  $\Delta r_i$  is a correction for the radial coordinate of the ith detector;

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 $\Delta t_{j}$ , j=1 to N, where  $\Delta t_{j}$  is a correction for the tangential coordinate of the jth detector; and  $\Delta \theta_{k}$ , k=2 to N, where  $\Delta \theta_{k}$  is a correction for the orientational coordinate of the kth detector.

12. The imaging method as described in claim 11, wherein the fitting parameters further include: positional coordinates of the point radiation source.

13. A method of PET imaging comprising:

- coincidence detecting radiation events from a calibration source with at least two detector heads;
- calculating correction factors that correct for mechanical misalignment of the detector heads from the coincidence detected calibration source radiation;
- during a diagnostic imaging procedure performed on a subject, generating image data in response to radiation collected with the detector heads;
- correcting the image data with the correction factors; and
- reconstructing the corrected image data into an image representation.

14. A coincidence imaging system comprising:

a gantry;

- a plurality of flat panel detectors disposed about the gantry;
- a data memory which stores measured data about radiation events detected by the detectors;
- a calibration memory which stores a plurality of calibration parameters for correcting data measured during a patient scan; and
- a processor in communication with the calibration memory and with the data memory which calculates the calibration parameters by a minimization

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algorithm that includes optimizing fitting parameters with respect to acquired radiation data associated with a point radiation source.

5 **15.** The imaging system of claim **14** wherein the minimization algorithm further includes:

calculating lines of response (LOR) based upon the fitting parameters and the measured data;

generating a figure of merit characterizing the apparent size of the point radiation source based upon the LOR's; and

optimizing the fitting parameters to produce a minimized figure of merit.

16. The imaging system of claim 15 wherein the calibration parameters include:

parameters relating to positional coordinates of the plurality of detectors.

17. The imaging system of claim 16, wherein:

the gantry is a rotatable gantry which acquires measured data over a range of gantry angular positions.

18. The imaging system of claim 14, wherein:

the figure of merit is generated by summing the square of a distance of closest approach of each LOR to a spatial point; and

the fitting parameters include the positional coordinates of the spatial point.

19. The imaging system of claim 14, wherein the generating of the figure of merit includes:

obtaining a crossing point of each pair of LOR's; and calculating a variance of the crossing points.

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20. The imaging system of claim 14, wherein the minimization algorithm further includes:

discarding measured data about radiation events whose energy is outside a preselected energy range.